

# Magnetic resonance imaging for jaw bone assessment: a systematic review

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## PECO QUESTION

“What is the diagnostic accuracy of magnetic resonance imaging for maxillary bone assessment, compared to reference-standard measurements?”

## METHODS

- (P) Population:** healthy maxilla and mandible sites.
- (E) Exposure:** magnetic resonance imaging (MRI).
- (C) Comparison:** reference-standard measurements (e.g. histology, physical measurements or computed tomography).
- (O) Outcome measures:** quantitative and/or qualitative bone histomorphometry measurements.
- (S) Studies:** diagnostic studies (e.g. experimental, observational, clinical, animal, in-vitro and ex-vivo design).

A detailed protocol was registered on PROSPERO (CRD42022342697).

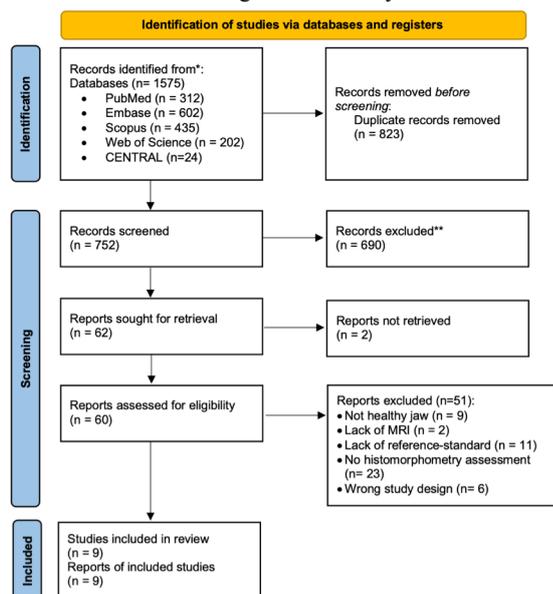
## RESULTS

### Characteristics of included studies

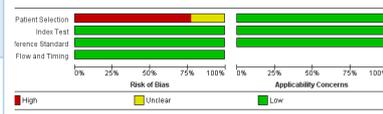
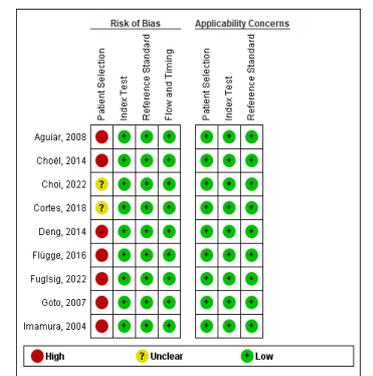
Author, year	Type of participants (n)	Evaluation site	Diagnostic purpose	Magnetic field and MRI device	MRI parameters	Reference test	No. of Examiners / experiences in radiology	Evaluated outcomes	Summary of outcomes
Aguilar, 2008	Dry cadaver (5)	Anterior mandible	Linear measurement for dental implant planning	1.0 T Sigma Contour (GE HealthCare)	T2-weighted images, ST 2mm, table feed 1 mm, TR/TE 112/3.5 ms, FOV 26 cm, matrix 256x256 pixels, scanning time 3 min.	CT and digital caliper	4 / specialists	Linear measurement (bone height)	There were no significant differences between the three tested groups (P=0.98).
Choi, 2014	Bone specimens (45) from fresh cadavers (15)	Anterior and posterior mandible	Trabecular bone assessment for determining optimal dental implant loading time	2T Oxford 85/310 magnet (Oxford) with a SMS console (MRS)	2D spin-echo sequence, TE/TR 21/550 ms, FOV ~30x15 mm <sup>2</sup> , ST 600 mm, matrix 256x128 pixels, in plane resolution > 110 mm, signal-to-noise ratio > 20, 40 averages, scanning time < 50 min.	DXA and bone densitometer	NR	DXA: bone mineral density; MRI: specific perimeter: ratio of bone perimeter and trabecular width.	Compared to female specimens, male specimens showed significantly higher values. The specimens from incisal regions showed the highest anisotropy.
Choi, 2022	Bone specimens (21) from patients (18)	NR	Evaluate bone marrow adipose tissue	14 T Magnex interfaced to a Bruker BioSpin (Billerica, MA)	3D gradient-echo sequence, TR/TE 48.6/2.6ms, matrix 256x256x256 pixels, scanning time ~14h.	CBCT and micro-CT	NR	MRI: BMAT content; Micro-CT: BV/TV; CBCT: radiodensity values.	The only statistically significant correlation (p 0.01) found was between micro-CT and 14 T MRI (r = 0.943).
Cortes, 2018	Bone specimens (7) from patients (7)	Mandible	BMF content assessment	15 T 130-mm horizontal bore magnet (Agilent, Yarnton)	3D gradient-echo pulse sequence, TE/TR 3.3/50 ms, receiver bandwidth 255-Hz, flip angle 25°, 16 averages, FOV 7.5x7.5x7.5 mm, matrix 128x128x128 pixels, voxel 59 μm, scanning time 32:07 min.	Micro-CT	2 / MRI analysis: PhD in oral radiology. Micro-CT: PhD student.	MRI: BMF; Micro-CT and MRI: BV/TV	Fat tissue volume and BV/TV had a significantly strong inverse correlation. There was high level of agreement between BV/TV calculated from MRI and micro-CT.
Deng, 2014	Fresh cadaver (1)	Posterior mandible	Mandibular nerve visualization and linear measurement to cortical bone	3 T Magnetom Trio (Siemens)	Fast gradient-echo sequence, TR/TE 2.3/3.67 ms, flip angle 10°, matrix 448x448 pixels, FOV 226x226 mm.	CT and digital caliper	NR	Linear measurement	No significant difference in average distance was reported between the three tested groups.
Flügge, 2016	Patients (2) and dry cadaver (1)	Posterior maxilla and mandible	Imaging exam for routine dental and maxillofacial diagnosis.	3 T TIM Trio (Siemens)	Gradient-echo fast low flip angle shots. In vivo, mandible: Matrix 64x64x28 mm, TE/TR 4.2/11 ms, flip angle 15°, three averages, scanning time 3:57 min. In vivo, maxilla: isotropic resolution 350 μm, FOV 34 cm <sup>2</sup> , TR/TE 12/4.8 ms, flip angle 15°, 5 averages, scanning time 6:40 min.	CBCT	2 / dentist > 5 years dedicated to radiology	Linear measurement	Except for bone measurements at 5mm, the majority of the bone measurement variations were statistically insignificant. The difference in mean measurements was not more than the method error.
Fuglsig, 2022	Cadaver specimens (12)	Posterior maxilla and mandible	Linear measurement (height and width)	9.4 T Bruker Biospec (Bruker Biospin)	Zero-Echo-Time sequence, FOV 75 mm isotropic, matrix 3663 pixels, image resolution 0.205 mm, flip angle 0.74°, projection under sampling of two, 50 averages, scan time 6 h	CBCT and histology	2 / dentist	Linear measurement	There was a significant agreement between CBCT, MRI, and specimens. MRI adequately exhibited hard and soft tissues
Goto, 2007	Patients (2), phantom (1), dry cadaver (1)	Anterior and posterior mandible	Linear measurement (distance between landmarks)	1.5 T Symphony (Siemens)	3D Vibe sequence. TR/TE 9.73/3.96 ms, flip angle 20°, voxel 0.7mm <sup>3</sup> , field of view 173x230mm, scanning time 6.5 min.	CT and micrometer	2 / trained observers	Linear and angle measurement	The correlation coefficient between MRI and direct osteometry was strong. MRI accuracy was comparable to CT accuracy.
Imamura, 2004	Patients (11)	Posterior mandible	Linear measurement	1.5 T (Shimadzu Corporation)	T1 weighted images, TR/TE 500/15 ms, FOV 150 to 260 mm, matrix 256x256, number of excitations twice, slice width 2.5 mm perpendicular to the dental arch and overlap 0.5 mm.	CT	2 / 4 years prosthodontist 27 years prosthodontist	Linear measurement and nerve detection	The canal's dimensional location in the second molar area was nearly similar with MRI and CT.

BV/TV, bone-volume-to-tissue-volume ratio; CBCT, cone beam computed tomography; CT, computed tomography; DXA, dual energy X-ray absorptiometry; FOV, field of view; NR, not reported; ST, slice thickness; T, Tesla; TE, echo time; TR, repetition time.

## PRISMA 2020 flow diagram for new systematic reviews.



## Risk of bias



## REFERENCES



## CONCLUSIONS

Despite jaw bone assessment is feasible with MRI, further studies and advancements are required to improve the applicability and usefulness.

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